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Graphic abstract 338x190mm (96 x 96 DPI)

1 The use of molecular descriptors to model pharmaceutical uptake by a fish primary 2 gill cell culture epithelium

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Elisabeth D. Chang¹, Christer Hogstrand^{1#}, Thomas H. Miller², Stewart F. Owen³, Nic R.
 Bury^{1,4}

- 6
- 1.King's College London, Department of Nutritional Sciences, Franklin Wilkins Building, 150
 Stamford Street, London, SE1 9NH, United Kingdom
- 9 2. King's College London, Department of Analytical, Environmental and Forensic Sciences,
- 10 Franklin Wilkins Building, 150 Stamford Street, London, SE1 9NH, United Kingdom
- 3. AstraZeneca, Global Safety, Health & Environment, Alderley Park, Macclesfield, Cheshire
 SK10 4TF, United Kingdom.
- 13 4. University of Suffolk, School of Science, Technology and Engineering, James Hehir
- 14 Building, University Quays, Ipswich, Suffolk, IP3 0AQ, United Kingdom.
- 15
- 16 # corresponding author
- 17 Email: christer.hogstrand@kcl.ac.uk

18 Abstract

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20 Modelling approaches, such as Quantitative Structure-Activity Relationships (QSARs) use 21 molecular descriptors to predict the bioavailable properties of a compound in biota. However, 22 these models have mainly been derived based on empirical data for lipophilic neutral 23 compounds and may not predict the uptake of ionizable compounds. The majority of 24 pharmaceuticals are ionizable and freshwaters can have a range of pH values that will affect 25 speciation. In this study we assessed the uptake of 10 pharmaceuticals (acetazolamide, 26 carbamazepine, diclofenac, beclomethasone, gemfibrozil, ibuprofen, ketoprofen, 27 norethindrone, propranolol and warfarin) with differing modes-of action and physicochemical 28 properties (pKa, logS, logD, logKow, molecular weight (MW) and polar surface area (PSA)) by an *in vitro* primary fish gill cell culture system (FIGCS) for 24 h in artificial freshwater. 29 Principal component analysis (PCA) and partial least squares (PLS) regression was used to 30 31 determine the molecular descriptors that influence the uptake rates. Ionizable drugs were 32 taken up by FIGCS and a strong positive correlation was observed between logS and a 33 negative correlation observed between pK_a , logD, MW and the uptake rate. This approach 34 shows that models can be derived based on physicochemical properties of pharmaceuticals 35 and using an *in vitro* gill system to predict uptake of other compounds. There is a need for a 36 robust and validated model for gill uptake that could be used in a tiered risk assessment to 37 prioritize compounds for experimental testing.

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40 Introduction

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Pharmaceuticals are biologically active molecules that have been detected in surface waters at ng to µg L⁻¹ concentrations¹ and are widely reported in aquatic fauna². The impacts associated with pharmaceutical exposure on aquatic organisms is unclear and knowledge is necessary to inform regulatory authorities and the pharmaceutical industry of compounds that may pose a risk³.

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48 As part of a chemical risk assessment it is necessary to determine the likelihood to 49 bioaccumulate. A bioconcentration factor (BCF) is a measure which includes uptake (k1) and 50 elimination rates (k2) and internal steady state concentration^{4, 5}. However, the uptake process, 51 along with metabolism, represent the largest factors of uncertainty in fish bioaccumulation 52 models^{6,7}, and BCF values for individual compounds derived from *in vivo* studies can vary 53 substantially⁸. Consequently, a novel approach to evaluating the bioavailability properties of a 54 chemical has been proposed which utilizes non-guideline methodologies in a tiered risk 55 assessment⁸. In this approach, in silico or in vitro data may be used in the lower tiers to assess 56 a chemical's bioavailability; if there is enough information to classify bioaccumulation potential 57 then a decision can be made as to whether further BCF studies are required⁸.

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59 Many mechanistic assessments of contaminant uptake are based on *in silico* models such as 60 Quantitative Structure-Activity Relationships (QSARs), that have largely been derived from data for lipophilic neutral compounds that passively diffuse across lipid membranes and 61 undergo little to no metabolism⁶. QSAR can include linear based estimations or more recently 62 63 machine learning applications such as neural networks and tree-based learning to predict organic chemicals bioconcentration⁹. However, an estimated 77.5% of pharmaceuticals are 64 65 ionizable¹⁰. Thus, the applicability of QSAR models developed on other contaminant classes (i.e. neutral hydrophobic contaminants) may be limited and inaccurately estimate the 66 67 accumulation of pharmaceuticals. For compounds that are ionizable the acid-base

68 dissociation constant (pK_a) describes the dissociation of the drug at a given pH and influences solubility, lipophilicity, permeability and protein binding¹¹. In the aquatic environment, surface 69 70 water pH will determine chemical speciation, and this is predicted to have an influence on 71 bioavailability¹². The typical pH of environmental water ranges between 6-9¹² although fish can 72 be found in bodies of water that are extremely acidic (pH 3)¹³ and highly alkaline (pH 10.5)¹⁴. The effect of pH on the toxicity¹² and uptake/elimination of ionizable compounds in fish has 73 been demonstrated¹⁵⁻¹⁷. Recently, Bittner et al.¹⁸ have demonstrated the impact of pH (5.5 – 74 75 8.6) on the uptake and toxicity of beta-blocker pharmaceuticals in zebrafish larvae; where the skin is likely to be the significant route of uptake. Karlsson et al.¹⁹ have examined the effect of 76 77 water and sediment pH (5.5 - 8.5 pH) on uptake of 3 pharmaceuticals uptake with a range of 78 pKa (4.01 – 9.62 pKa) in the freshwater oligochaete *Lumbriculus variegatus*.

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80 There is a desire towards the development of *in vitro* models to replace or supplement current 81 animal experimental procedures²⁰, in accordance with the replacement, reduction, and 82 refinement (3Rs) principle²¹. This is also reflected in European legislature that states non-83 animal alternative approaches should be used in place of animal procedures wherever 84 possible. A fish gill cell culture system (FIGCS) was developed using primary fish cells that has shown promise as an alternative system for whole fish chemical uptake studies²². FIGCS 85 86 maintains many of the characteristics of the in vivo epithelium, including the presence of multiple cell types associated with transport of ions across the gills and the ability to tolerate 87 freshwater water application to the apical surface. The in vitro data obtained from FIGCS 88 experiments has the potential to be an important component of the lower tier in a tiered testing 89 90 system⁸ as the gills are a primary route of uptake in fish²². It has recently been used to investigate the absorption of 7 pharmaceuticals with a similar pK_a of 8.1 to 9.6 across the gill²³. 91

92

93 There is a paucity in fish pharmaceutical uptake and BCF values because the tests to derive 94 these use a large number of organisms, are time consuming and expensive to conduct. In this 95 study we assessed the uptake of 10 pharmaceuticals by an *in vitro* fish gill model with differing

96 physiochemical properties and there were three aims. Firstly, to assess the uptake of ionizable pharmaceuticals by this fish gill epithelium. Secondly, to demonstrate how an *in vitro* epithelial 97 98 model can be used to evaluate the propensity for a drug to enter a fish from the water and how this information could form part of a tiered risk assessment approach^{8,24}. Thirdly, Lipsinki 99 100 et al.²⁵ proposed that the molecular properties (molecular weight, hydrogen bond donors and 101 acceptors and $\log K_{ow}$) of a chemical can be used as a screening tool to determine the 102 likelihood of absorption across a membrane, we extended this concept and used the 103 pharmaceutical molecular descriptors and partial least squares (PLS) regression analysis to 104 model uptake rate and identify those descriptors that influence gill uptake. We were able to 105 show that solubility, pKa, octanol-water distribution coefficient and molecular weight are the 106 most important descriptors driving epithelial drug uptake rates.

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108 Materials and Methods

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110 Fish gill cell culture system (FIGCS)

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Juvenile rainbow trout (*Oncorhynchus mykiss*) were obtained from a local trout farm and housed in dechlorinated-aerated City of London tap water ($[Na^+]=0.53$ mM, $[Ca^{2+}]=0.92$ mM, $[Mg^{2+}]=0.14$ mM, $[K^+] = 0.066$ mM and $[NH_{4^+}] = 0.027$ mM). Temperature was maintained at 14°C with a 14h light:10h dark cycle and fish were fed a 1% (w/v) ration of trout pellets daily.

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Primary fish gill cell culture inserts were prepared in companion wells and maintained according to protocols described in Schnell et al.²². The transepithelial resistance (TER) was monitored daily using an epithelial tissue voltohmmeter (EVOMX) with STX-2 chopsticks (World Precision Instruments). A TER value of above 3,000Ω cm⁻² was used as criteria for the presence of a tight epithelium, as previously determined using ¹⁴C-mannitol as a paracellular
 permeability marker²³.

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125 Pharmaceuticals exposures and cell viability assay

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127 Analytical grade pharmaceuticals (purity \geq 97%) from differing classes of action with differing 128 chemical properties (Table 1) were purchased from Sigma Aldrich, and included 129 acetazolamide (CAS: 59-66-5), beclomethasone (CAS: 4419-39-0), carbamazepine (CAS: 130 298-46-4), diclofenac sodium salt (CAS: 15307-79-6), gemfibrozil (CAS: 25812-30-0), 131 ibuprofen sodium salt (CAS: 31121-93-4), ketoprofen (CAS: 22071-15-4), norethindrone-19 132 (CAS: 68-22-4), propranolol hydrochloride (CAS: 318-98-9) and warfarin (CAS: 81-81-2). 133 Pharmaceutical stocks were prepared at a concentration of 1 mg mL⁻¹ in methanol or ethanol 134 and stored at -80°C.

135

136 Following formation of a tight epithelium inserts were prepared for exposure by washing with 137 phosphate buffered saline. The apical freshwater (AFW) used for apical exposure was 138 prepared according to OECD₂₀₃ Test Guidelines²⁶ (2 mM CaCl₂; 0.5 mM MgSO₄; 0.8 mM 139 NaHCO₃, 77.1 µM KCI, with a measured pH 7.6) with individual pharmaceuticals added at a 140 concentration of 1 µg mL⁻¹, which is equivalent to: 450 nM acetazolamide, 245 nM beclomethasone, 423 nM carbamazepine, 338 nM diclofenac, 399nM gemfibrozil, 485 nM 141 ibuprofen, 393 nM ketoprofen, 355 nM norethindrone, 386 nM propranolol, and 324 nM 142 warfarin. To expose cells 1.5 mL of exposure water was added to the apical compartment and 143 2 mL of L15 media with 5% FBS to the basal compartment. The inserts, and 1.5 mL exposure 144 water samples (T₀) were incubated at 18 °C in the dark for 24 hrs. In the case of the T₀ samples 145 this was to assess if the compounds remained stable over the 24 hrs exposure period at 18°C 146 147 in the absence of cells. The T₀ and the 1.5 mL apical compartment water samples after 24 hrs exposure (T₂₄) were collected and stored at -80°C for further analysis. Measurements were 148

made on 4 inserts derived from 2 to 3 biological replicates, with each biological replicatecomprising of cells harvested from 2 fish.

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152 To consider the adhesion of the compounds to the companion well and insert membrane 153 during 24 hrs of exposure, a cell-free experiment was performed. To assess pharmaceutical 154 toxicity, single seeded primary gill cells were grown in T75 flasks to 80% confluent, then 155 trypsinized and transferred to 96-well at a density of 1x10⁵ cells well⁻¹. Twenty-four hours post-156 seeding in the 96-well plates cells were exposed to pharmaceuticals at 1 µg mL⁻¹ in L15 with 157 5% FBS for 24 hours, after which a MTT viability assay 3-(4,5-dimethylthiazol-2-yl)-2,5diphenyltetrazolium bromide) was performed following methods adapted from Riss et al.²⁷. pH 158 159 stability of the AFW with 1µg ml⁻¹ of compound was measured with and without cells and found 160 to be stable over a 24 hour period.

161 HPLC Analysis

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For HPLC analysis individual T₀ or T₂₄ samples were pooled into three separate mixtures: Mix 163 164 A included beclomethasone, ibuprofen and warfarin, Mix B included carbamazepine, diclofenac, gemfibrozil, ketoprofen and norethindrone and Mix C included acetazolamide and 165 propranolol for solid phase extraction (SPE) with Oasis HLB cartridges (200mg sorbent, 6cc). 166 167 Cartridges were initially conditioned with 6 mL methanol (HPLC grade) followed by 6 mL water 168 (HPLC grade) then loaded with either pooled sample Mix A, B or C. Cartridges were washed 169 with 4 mL water, dried under vacuum pressure and eluted with 6 mL methanol or stored at -170 80°C for later elution. Samples were then dried under nitrogen at 45°C for 80 min (Biotage 171 TurboVap), reconstituted in 500 µL 90:10 (v/v) water:acetonitrile and vortexed for 2 minute 172 before transfer to amber HPLC vial for analysis.

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174

Liquid chromatography was performed on an Agilent 1260 Infinity series LC system using a
 Waters Sunfire C₁₈ column (100 Å, 3.5 μm, 4.6 mm x 150 mm) at a flow rate of 0.2 mL min⁻¹

177 and injection volume of 20 µL. Mobile phase A and B consisted of HPLC grade water and HPLC grade acetonitrile, respectively, with initial running conditions of 10% phase B at a 178 179 column temperature of 40 °C. The gradient elution was as follows; linear ramp with phase B 180 increased to 80% at 12 min, held for 13 min, then returned to initial conditions at 28 min. Total 181 run time was 40 min including a 12 min re-equilibration period. An Agilent 1290 Infinity Diode Array Detector was used for detection of diclofenac and warfarin at 214 nm; carbamazepine, 182 183 ibuprofen and gemfibrozil at 220 nm; beclomethasone and propranolol at 230 nm; 184 norethindrone at 254 nm; ketoprofen at 263 nm and acetazolamide at 273 nm.

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Method performance was assessed by matrix-matched calibration curves generated for the AFW. Method linearity (5 concentrations, n=3) was determined from 0.5 -2.5 μ g mL⁻¹ and signal to noise ratio of 3:1 and 10:1 of low concentration spiked samples was used to determine the LOD and LOQ, respectively (n=6). Precision was determined using spiked samples at 1 μ g mL⁻¹(n=6) and accuracy was determined using spiked samples and values from method linearity (n=6). Recovery was assessed by comparing spiked samples (preextraction) to post-extract spiked samples at a concentration of 0.5, 1 or 2 μ g mL⁻¹ (n=3).

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194 Estimation of Gill Uptake Rates

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Primary gill cell culture pharmaceutical uptake was calculated based on the loss of compound
from the apical compartment corrected for the amount that adhered to the polystyrene plastic
of the companion wells and inserts without cells over 24 hrs (Equation 1).

199

200 Uptake rate (nmol cm⁻² h⁻¹) =
$$(T_0 - T_{24}) - (T_0^p - T_{24}^p)$$
] / (t x cm²) Eqn. 1
201

Where T_0 and T_{24} represents the moles (nmoles) of drug present in the apical compartment in the presence of cells at 0 and 24 hrs, respectively, and T_{0^p} and T_{24^p} represent the moles of drug present in the apical compartment in the absence of cells at 0 h and 24 h, respectively; t= time of the flux measurement (24 hrs) and cm² represents the surface area of the epithelium (0.9 cm²). Sorption controls (inserts and exposure media only) were setup to account for any losses of compound through volatilization, sorption to plastics and any other degradative processes. Insert controls showed that these processes were negligible and therefore in the presence of cells disappearance of compound is related to the uptake of the compound into the gill epithelium and transfer across into the basolateral layer over 24 hours.

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212 Statistics and Modelling Approaches

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214 A one-way ANOVA followed by a Tukey's post hoc test was performed to compare the uptake 215 rates of each compound using GraphPad Prism 6.0. Modelling approaches used 6 molecular 216 descriptors (Table 1) including; the acid dissociation constant (pK_a), the octanol water 217 distribution coefficient at pH 7.4 (logD), the octanol-water partition coefficient (log K_{ow}), polar 218 surface area (PSA) and molecular mass (M_w). The two descriptors log K_{ow} and logD are both 219 measures of hydrophobicity, but logD takes into account both neutral and ionizable species at 220 a given pH whereas $\log K_{ow}$ only takes into account the neutral fraction. Principle component 221 analysis (PCA) and partial least squares (PLS) regression were performed using the R 222 statistical computing language, R version 3.4.3 (freely available at https://www.r-project.org/). 223 All scripts were written with RStudio (freely available at https://www.rstudio.com/), packages 224 used for PCA and PLS analysis were stats and plsdepot, respectively. Full dataset used in 225 modelling, latent variable scores, loadings, weights and cross-validation of models are given 226 in the SI (Figure S3 and Tables S4-S7). For cross-validation of the PLS model, a leave-one-227 out approach was used.

228

229 Results

Cell viability was assessed by MTT assay and none of the pharmaceuticals at a concentration
of 1 µg mL⁻¹ showed signs of cytotoxicity (Supporting Information (SI), Figure S1) and HPLC
method performance assessment is provided in the supplementary data (SI Table S1 and S2).

235 Pharmaceutical adhesion to the companion wells over 24 hrs was between 0.7 to 5% (data 236 not shown) and was taken into consideration when calculating uptake rates. Acetazolamide 237 uptake $(0.125 \pm 0.032 \text{ nmoles cm}^{-2} \text{ h}^{-1})$ was significantly greater than beclomethasone, 238 carbamazepine, diclofenac and norethindrone (beclomethasone 0.021 ± 0.015 nmoles cm⁻² h 239 ¹, carbamazepine 0.022 \pm 0.004 nmoles cm⁻² h⁻¹, norethindrone 0.024 \pm 0.003 nmoles cm⁻² 240 h^{-1} , diclofenac 0.027 ± 0.003 nmoles cm⁻² h^{-1}) (Figure 1). The other ionizable drugs, except for 241 diclofenac, showed higher, but not significantly higher uptake rates (ibuprofen 0.072 ± 0.013 242 nmoles cm⁻² h⁻¹, gemfibrozil 0.075 \pm 0.007 nmoles cm⁻² h⁻¹, ketoprofen 0.061 \pm 0.006 nmoles 243 cm⁻² h⁻¹, propranolol, 0.095 \pm 0.026 nmoles cm⁻² h⁻¹ and warfarin 0.070 \pm 0.012 nmoles cm⁻² 244 h⁻¹) compared to the neutral drugs, beclomethasone, carbamazepine, and norethindrone (Figure 1, and SI Figure S2). 245

246

Modelling of the molecular descriptors was performed using PCA analysis to identify 247 248 compound similarity (Fig 2). The first two principal components explained a cumulative variance of 69% (PC1 = 48%, PC2 = 21%) in the descriptor space. The score plot indicates 249 250 that there were no apparent outliers in the dataset. Clustering of compounds was minimal but 251 was expected with the low number of cases available for modelling (n=10). The largest 252 variation in the descriptor space was observed for the compound beclomethasone (Fig. 2). 253 The variance of this case can be explained in terms of the loadings, where this compound was 254 the largest (MW = 408.92) and most hydrophobic (logD = 4.16) of all compounds that were 255 tested. From the descriptor loadings, logS and MW were negatively correlated with each other. 256 The loadings for the first latent variable also showed that logD (0.567), MW (0.505), logS (-257 0.444) and p K_a (0.407) were more important variables than log K_{ow} (0.201) or PSA (0.146).

PLS was implemented to interpret molecular descriptors that influence gill uptake rates ofpharmaceuticals and enable a predictive modelling approach with:

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262	Uptake Rate (nmoles cm ⁻² h ⁻¹) = $1.23E-01 + (-1.59E-03 \times pK_a) + (1.53E-02 \times logS) + (-7)$	26E-
263	03 x logD) + (9.15E-03 x logK _{ow}) + (-9.48E-05 x MW) + (3.83E-04 x PSA)	Eqn.
264	2	

265

The adjusted correlation coefficient (R²_{adj}) and the cross-validated R² (Q²) of the PLS 266 267 regression model was 0.7863 and 0.5397, respectively. No cases were observed as outliers in the PLS model determined by the Hotelling's T² 95% confidence ellipse (data not shown). 268 269 Based on the cumulative Q² statistic (see SI Figure S4), the optimal number of latent variables 270 for the PLS model was two. The loadings plot (Figure 3a) indicated that logS was positively correlated with gill uptake whereas logD, pK_a and MW were negatively correlated with gill 271 272 uptake. The logKow and PSA descriptors were relatively less important for modelling gill uptake 273 when compared with the previously mentioned descriptors. The use of PLS to predict gill 274 uptake showed good performance with the mean absolute error of 0.01 ± 0.01 nmol cm⁻² h⁻¹ 275 (MAE±SD) for all compounds tested. Larger inaccuracies in the predictions were observed for 276 the four compounds; carbamazepine (122%), diclofenac (61%), norethindrone (35%) and 277 propranolol (32%) (Fig 3b and c).

278

279 Discussion

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The uptake rate of 10 pharmaceuticals by a fish primary gill cell culture system was assessed. From our dataset we were able to demonstrate that a PLS regression model based on the drug molecular descriptors could be developed for pharmaceutical uptake rate by this epithelium, with LogS, pK_a , logD and MW found to be the most important descriptors driving epithelial drug uptake rates.

The uptake rates of the compounds from the apical compartment reflect the apparent epithelial permeability (P_{app}) of the compound by the FIGCS cells. The P_{app} can be expressed as an equation (equation 3) and takes into consideration four factors: partitioning in the aqueous boundary layer (P_{ABL} , ABL), adhesion to filter insert (P_f) and transcellular (trans) or paracellular (para) transfer (P_{trans} , P_{para})²⁸. The aqueous boundary layer is assumed to have a distinct boundary with the bulk water adjacent to both sides of the membrane²⁹.

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295

296

$$\frac{1}{P_{app}} = \frac{1}{P_{ABL}} + \frac{1}{P_f} + \frac{1}{P_{trans} + P_{para}}$$
Eqn. 3

297 Two of the four factors can be discounted, due to the nature of the system. Firstly, adhesion 298 to plastic (P_f) and inserts was taken into consideration when calculating the uptake rate. 299 Secondly, a previous study conducted using the paracellular marker ¹⁴C-mannitol determined 300 that at TER values above $3,000\Omega$ cm² the FIGCS were relatively impermeable to the marker 301 and indicated that transport was via transcellular routes²³, all compounds in the current study 302 have a greater molecular weight than mannitol thus paracellular transfer (P_{para}) was negligible. 303 Thus, the uptake rates reflect partitioning in the ABL (P_{ABL}), uptake into cells and across the 304 basolateral membrane (P_{trans}) into the basolateral compartment, in addition to any potentially 305 metabolized compound efflux from the gill cells back into apical compartment.

306

307 All uptake studies were conducted in AFW and under these conditions acetazolamide (71.5%), 308 diclofenac (100.0%), gemfibrozil (99.9%), ibuprofen (99.8%), ketoprofen (99.9%), propranolol 309 (98.5%) and warfarin (99.7%) are all predicted to be ionized (% ionized in parentheses), 310 whereas beclomethasone, carbamazepine, and norethindrone are not ionized. All ionizable drugs, except diclofenac, showed higher permeation into the primary gill cell epithelium when 311 312 compared to the neutral drugs (Figure 1). The observation that ionizable drugs are capable of 313 permeating the gill epithelium corroborates a previous study in FIGCS concerning the uptake of a set of pharmaceuticals with pK_a between 8.1-9.6²³ and a number of studies suggest that 314 315 ionizable compounds can be taken up by the fish gill^{e.g. 15,16,18,19,23,30,31}. The uptake of 9 weakly

316 acidic chlorinated phenols by rainbow trout did not vary between pH 6.3 to 8.4 despite the proportion of the compounds ranging in ionization from 1 to 99 %¹⁵, the accumulation of the 317 weak basic diphenhydramine (p K_a 9.1) at 10 µg L⁻¹ reached steady state in fathead minnow 318 at pH 7.73 and 8.63 after ~24 h and only at pH 6.87 was accumulation greatly reduced³¹ and 319 320 ionizable surfactant³², perflouroakyl acids³³ as well as phenols and carboxylic acids³⁴ have been observed to cross the gills of fish. However, membrane permeation may be an order of 321 magnitude less than for the neutral form³⁰. Erickson et al.,¹⁶ developed a mechanistic model 322 323 of ionized organic chemical uptake at the fish gill which expanded on an original model for 324 unionized chemical uptake^{35,36}. This new model included a factor that takes into account the 325 ability of the fish to alter the pH adjacent to the apical membrane and thus generating a 326 microclimate that differs to the bulk water³⁷. These changes in pH at the gill surface helped to 327 explain uptake of diphenylamine³¹ and the chlorinated phenols^{15,16}. However, in the current 328 study uptake of the acidic and basic pharmaceuticals showed similar uptake rates, and if 329 uptake is solely due to the neutral form of the drug, then pH of the culture epithelial microclimate would have to be in the region of pH 3 to ensure the weakly acidic drugs ($pK_a 4$ 330 331 -5.08) were unionized. It is also unlikely that uptake is solely due to the ionized form because 332 the basic drugs show similar uptake rates (Figure 1 and ²³). In contrast to the other ionizable 333 compounds, diclofenac is the only drug that exhibited a relatively lower uptake rate. It is 334 unclear why this may be, but of the drugs used in the current study the structure of diclofenac 335 is more complex containing both an amine and carboxylic acid group and lacks conformational 336 flexibility³⁸ that may influence transport by the gill epithelium.

337

The PLS modelling approach showed that all descriptors here have an influence on the uptake rate but more of the explained variance was correlated to the logS, logD, pKa and MW descriptors. The regression model (Equation 2) showed a good potential to predict uptake rates in the FIGCS system at the tested concentration and water chemistry ($r^2 = 0.786$). Modelling is an important aspect to understanding fate of pharmaceuticals in the aquatic environment and these approaches are complementary to *in vitro* systems for the replacement

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344 of animal testing. Comparison to *in vivo* fish uptake rates would be useful, however there are 345 a limited number of studies reporting these values. We have collated those 'steady state' 346 plasma concentrations for 9 of the 10 pharmaceuticals in the supplemental file (SI Table S8), 347 but note that the complexity and variation in pH, exposure, species, size and temperature 348 make direct comparison to our data difficult. Furthermore, these studies do not allow us to 349 derive uptake rates and therefore are not suitable for comparison with our dataset. Predicted 350 K₁, LC₅₀ and BCF values can be derived from QSAR models for fish (SI, Table S8). However, 351 a poor correlation was observed between the predicted K₁, LC₅₀ and BCF and our *in vitro* 352 pharmaceutical uptake rates (Table S8), emphasizing the need for alternative models for these 353 compounds. To fully validate the model a much larger number of compounds would be 354 needed. A robust and validated model for gill uptake could then be used as a pre-screen to 355 prioritize compounds for experimental testing in a tiered approach⁸. In this scenario if a 356 compound is predicted to not be bioavailable in *in vitro* studies and other information from 357 lower tier screens support this observation, then further BCF testing in living fish may not be 358 required^{8,24}.

359

360 The pharmaceutical uptake rate was most strongly positively correlated to logS (Figure 2b) 361 suggesting that this physiochemical property facilitates access of the pharmaceuticals to the 362 cells and uptake. The ABL in multi-well plates is between 1,000 - 2,000 µm and forms a significant diffusional barrier³⁹ where by the concentration in bulk solution exceeds that located 363 364 at the membrane surface. Increased solubility aids permeability across the ABL²⁹ allowing for greater interaction with the membrane⁴⁰. Carbamazepine was expected to have a higher 365 366 uptake based on solubility, as well as being neutral and hydrophobic, but influx rates were low 367 and carbamazepine had the largest prediction inaccuracy in the PLS regression model. The reason for this is uncertain. Carbamazepine has a low BCF value in adult zebrafish (BCF_{ss} of 368 $1.41 \pm 7.13 \text{ L kg}^{-1}$) but this is likely associated with greater biotransformation capacity and 369 370 clearance rather than a significant reduction in uptake when compared to other pharmaceutical 371 and personal care products tested¹⁷. Whether the gills actively excrete carbamazepine back into the apical water compartment remains to be determined. Carbamazepine's mode of action is promiscuous, and it interacts with different types of receptors and channels⁴¹. However, the main target is voltage gated Na⁺ channels located on the surface of the cells⁴¹ where it acts as a competitive inhibitor by allosteric inhibition⁴². A possibility is that in our system the drug adheres to and interacts with the surface and related channels but does not permeate into the cell.

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379 A negative correlation of uptake rates with logD was observed. The gill membrane consists of 380 a range of phospholipids (e.g. phosphatidylethanoilamines and phosphatidylcholine) with 381 differing properties capable of forming electrostatic and hydrogen bonds with charged 382 molecules. It has been shown that ionized drugs can partition into artificial lipid membranes 383 greater than predictions based on $\log K_{ow}^{44}$ and there is a positive relationship between the 384 dipole potential in the region between the aqueous phase and the interior membrane bilayer 385 allowing permeation of ionized compounds in these synthetic membranes^{24,45,46}. This 386 phenomenon gave rise to the pH-piston hypothesis to explain sorption of ionized drugs into 387 artificial vesicles consisting of dioleylphosphatidylcholine, due to electrostatic interactions with 388 acidic and basic drugs⁴⁵ and may explain how the ionized compounds are able to cross the 389 membrane.

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The PLS regression also indicated that the uptake rates were negatively correlated with MW. MW is known to play a distinct role in cellular uptake of solutes and has been used successfully to model permeability of both neutral and charged molecules, in addition to be a component of Lipinski's rule of 5 in drug discovery^{43,47,48}. The LogK_{ow} and PSA accounted for some of the variance in the regression but to a much less extent than the other molecular descriptors.

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The role of transport proteins in ionizable drug uptake is axiomatic^{e.g. 49-51}, but the extent of the role transport proteins play in drug uptake is debated. Kell and colleagues proposed that uptake is almost solely due to transport proteins⁵², though this has been strongly questioned⁵³. 400 In our current study all flux rates were measured at concentrations that far exceed 401 environmental concentrations and it is likely that carrier mediated transport processes were 402 saturated. Here we are measuring both the passive and facilitated uptake, with passive 403 dominating and entry likely via electrostatic interactions with the phospholipid membrane of 404 the fish gill²⁴. But, several organic, anion, cation or zwitterion transporters are present at the gill e.g. *slco1d1*⁵⁵, OATP⁵⁶ and *slc15a2*⁵⁷, and their ability to facilitate drug uptake from the 405 406 water requires further understanding. An alternative explanation for the uptake of charged 407 molecules is transportation as ion pairs⁵⁸, a property that has been utilized to assist in 408 developing drug penetration for a number of epithelia, such as the ocular epithelium⁵⁹ and the 409 skin⁶⁰, but has not been considered for fish gill epithelial. Natural water contains numerous 410 potential counterions and the fish excretes ions and other charged molecules from the gill that 411 could form ion-pairs with charged drugs.

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413 Environmental Implications

414 The current study shows that the FIGCS can be used to assess drug uptake by fish gills from 415 the water in accordance with previous studies²³. It also shows that ionizable drugs are able to 416 cross the gill epithelium, but further work is required to ascertain the significance of the gill 417 microclimate at the apical membrane, ion pairing, electrostatic interactions (between the 418 ionized pharmaceutical and the membrane phospholipids) and transport proteins on ionizable 419 compound transport. A PLS regression model based on the physicochemical properties of the 420 drug was used to predict uptake rate (the model accounted for 78% of the explained variance) where logS, pK_a , logD and MW were significant drivers. To fully validate the model a much 421 422 larger number of compounds would be needed, however, this approach shows that modelling 423 can be used to understand the uptake of pharmaceuticals by an *in vitro* epithelium system that 424 could replace whole animals in bioaccumulation studies. There is a need a robust and 425 validated model for gill uptake could then be used as a pre-screen to prioritize compounds for 426 experimental testing in a tiered risk assessment⁸ where compounds that do not cross the gill 427 epithelia may not need further costly and time-consuming animal testing.

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442 Supporting Information.

- Cytotoxicity of the pharmaceuticals in primary gill cells (MTT assay)
- *in vivo* BCF data from literature
- QSAR predictions of K₁, LC₅₀ and BCF
- HPLC method performance assessment
- Linear regression analysis of uptake rates in relation to the chemical descriptors
- 448 modelling supplementary information including scores, loadings, modified weights and 449 cross-validation for PCA and PLS.

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- 620 with pene 621 1557.

Table 1: Pharmaceutical molecular descriptors.

			Molecular				%
	р <i>К</i> а	logS	Weight (g mol ⁻¹)	logD	logK _{ow}	PSA (Ų)	ionisation at pH 7.6
Acetazolamide	7.20	-2.36	222.24	0.23	3.48	115.04	71.5
Beclomethasone	13.85	-5.4	408.92	4.16	3.49	106.97	0
Carbamazepine	15.96	-3.2	236.27	2.28	2.28	46.33	0
Diclofenac	4.00	-4.8	296.15	1.22	1.9	52.16	100
Gemfibrozil	4.42	-4	250.33	1.40	4.77	46.53	99.9
Ibuprofen	4.91	-3.5	206.28	0.29	2.48	40.10	99.8
Ketoprofen	4.45	-4.1	254.28	0.06	0.97	54.37	99.9
Norethindrone	17.59	-4.7	298.40	2.98	3.15	37.30	0
Propranolol	9.42	-3.5	259.34	1.29	3.09	41.49	98.5
Warfarin	5.08	-3.8	308.32	0.16	0.85	63.60	99.7

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Figure 1: Pharmaceutical uptake rate into the fish gill cell culture system. Values represent average of 4 inserts derived from between 4 -6 fish. Bars with differing letters are significantly different from each other when compared via a One-way ANOVA followed by a Tukey's posthoc test, p<0.05.

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Figure 2: PCA biplot showing the first two principal component (PC1 and PC2) loadings and
scores for each molecular descriptor and case, respectively. Scores are indicated on the first
axes (left and bottom, black) loadings are indicated by the second axes (right and top, red). A
-acetazolamide; B – beclomethasone; C- carbamazepine; D – diclofenac; G – gemfibrozil; I –
ibuprofen; K - ketoprofen; N – norethindrone; P – propranolol and W – warfarin.

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Figure 3: PLS regression analysis showing (A) loadings of the first two latent variables for molecular descriptors (independent variables) and uptake rate (dependent variable) (B) predicted versus observed gill uptake rates using PLS regression model (C) raw residuals of predicted uptake rates.





663 Figure 2



